Medical Image Analysis

CS 778 / 578

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Outline

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Outline

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- [Image smoothing](#page-4-0)
- 2 [Isotropic Diffusion Formulation](#page-14-0)

Intro

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Using sliding windows for image processing

Intro

Figure: Pixel [i,j] in the output image (shown in red) depends on the pixels in the neighborhood of [i,j] in the input image (shown in blue).

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Image smoothing

We can compute several things within each window:

- Local averaging : mean
- Weighted local average : weight the center pixel higher
- Nonlinear filtering : median
- We can look at larger neighborhoods : 5×5 , 7×7 and larger.
- Why are these odd dimensions?
- In 3D : $3 \times 3 \times 3$ neighborhoods and larger.

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Intro Image smoothing

Local averaging

We associate weights, *wkm* with each voxel in the sliding window:

The new intensity, $g(i,j)$, computed from from the original image, f, and the weights, w

$$
g(i,j) = \sum_{m=-1}^{1} \sum_{k=-1}^{1} w_{km} f(i+k, j+m)
$$

is the mean of intensity values within the sliding window.

When applied to the whole image we write $g = w \otimes f$ (This is also referred to as 'convolution')

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Local averaging results

- Edges are destroyed.
- Smoothing is a low-pass filtering operation.
- High frequency components are attenuated, low frequency components of the image are preserved.

It can be shown that if image f is corrupted by additive Gaussian noise of variance σ_f^2 then the variance of the noise on image g is

$$
\sigma_g^2 = \sum_{m=-1}^1 \sum_{k=-1}^1 w_{km}^2 \sigma_f^2
$$

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Fourier transform

Transform from time/space domain to frequency domain Denoted $\mathcal{F}[f] = \hat{f}$

Some calculations are simpler in frequency domain:

 $\mathbb{R}^n \times \mathbb{R}^n \xrightarrow{\sim} \mathbb{R}^n \times \mathbb{R}^n$

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Fourier Transform - Convolution Theorem

The continuous definition of convolution

$$
f * g = \int_{-\infty}^{\infty} f(\tau)g(x - \tau) d\tau
$$
 (1)

$$
\mathcal{F}[f * g] = \int_{-\infty}^{\infty} \left[\int_{-\infty}^{\infty} f(\tau)g(x - \tau) d\tau \right] e^{-2\pi i kx} dx \tag{2}
$$

Using the fact that $e^x = e^{\tau} e^{x-\tau}$

$$
\mathcal{F}[f * g] = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} [e^{-2\pi ik\tau} f(\tau)][e^{-2\pi ik(x-\tau)}g(x-\tau)] dx d\tau \qquad (3)
$$

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Intro Image smoothing

Substituting $y = x - \tau$, and $dy = dx$

$$
\mathcal{F}[f * g] = \int_{-\infty}^{\infty} e^{-2\pi i k \tau} f(\tau) d\tau \int_{-\infty}^{\infty} e^{-2\pi i ky} g(y) dy \tag{4}
$$

$$
\mathcal{F}[f * g] = \mathcal{F}[f]\mathcal{F}[g] \tag{5}
$$

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- Convolution can be implemented as multiplication in the frequency domain.
- Gaussian convolution is Gaussian multiplication in frequency domain.
- Gaussian convolution is low-pass filtering.

Image Gradient

$$
\nabla I(x, y) = \begin{bmatrix} \frac{\partial I}{\partial x} \\ \frac{\partial I}{\partial y} \end{bmatrix}
$$
 (6)

Vector points in the direction of fastest increase in $I(x, y)$

- Edges are discontinuities in intensity
- ||∇*I*|| is the edge "strength" (sharpness of the edge)
- \bullet ∇I is perpendicular to the edge

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Edge detection using the gradient

(http://amath.colorado.edu)

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Intro Image smoothing

Divergence

For the vector-valued function
$$
\mathbf{V}(\mathbf{x}, \mathbf{y}) = \begin{bmatrix} v_1(x, y) \\ v_2(x, y) \end{bmatrix}
$$
 the divergence is defined as

$$
\operatorname{div} \mathbf{V}(\mathbf{x}, \mathbf{y}) = \frac{\partial v_1}{\partial x} + \frac{\partial v_2}{\partial y} \tag{7}
$$

More notation:

 $\text{div}(\nabla I) = \nabla \cdot \nabla I = \nabla^2 I$ (the Laplacian)

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Divergence of a vector field

$$
\operatorname{div} \mathbf{V}(\mathbf{x}, \mathbf{y}) = \frac{\partial v_1}{\partial x} + \frac{\partial v_2}{\partial y} \tag{8}
$$

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Physical interpretation : sources or sinks a velocity field.

$div V > 0$ (left), $div V < 0$ (right)
Image from "The idea of divergence and curl"

(http://www.math.umn.edu)

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Outline

2 [Isotropic Diffusion Formulation](#page-14-0)

- [Description](#page-15-0)
- [Solution](#page-16-0)

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Let image =
$$
I(x, y, z, t)
$$
.

$$
\frac{\partial I}{\partial t} = \text{div}(\nabla I) \tag{9}
$$

- The equation describes the way physical systems achieve equilibrium.
- When describing heat transfer, $I(x)$ is temperature.
- When describing diffusion, $I(x)$ is molecular concentration.

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Solving the heat equation

In one dimension:

$$
\frac{\partial I}{\partial t} = \frac{\partial^2 I}{\partial x^2} \tag{10}
$$

Take the Fourier transform of both sides

$$
\mathcal{F}\left[\frac{\partial I}{\partial t}\right] = \mathcal{F}\left[\frac{\partial^2 I}{\partial x^2}\right] \tag{11}
$$

Let $\mathcal{F}[I(x,t)] = U(\omega, t)$ and

Recall that

if
$$
f(x) \leftrightarrow F(\omega)
$$
,
then $f'(x) \leftrightarrow i\omega F(\omega)$, and
 $f''(x) \leftrightarrow -\omega^2 F(\omega)$

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$$
\frac{\partial U(\omega, t)}{\partial t} = -\omega^2 U(\omega, t) \tag{12}
$$

with initial conditions

$$
U(\omega, 0) = U_0(\omega) \tag{13}
$$

You can verify that

$$
U(\omega, t) = U_0(\omega)e^{-\omega^2 t}
$$
 (14)

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Is a solution to the problem.

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Taking the inverse Fourier transform

$$
\mathcal{F}^{-1}[U(\omega, t)] = \mathcal{F}^{-1}[U_0(\omega)e^{-\omega^2 t}]
$$
\n(15)

we see that

$$
I(x,t) = I_0(x) * e^{-\frac{x^2}{2\sigma_t^2}}
$$
 (16)

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where $\sigma_t^2 = 2t$

This is Gaussian convolution

- \bullet Evolving $I(x)$ according to the heat equation is equivalent to convolving with a Gaussian kernel.
- Longer evolution corresponds to convolution with Gaussians of higher variance.
- This gives us firm footing for studying PDEs in the context of image processing.

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Next Class

Variational calculus. Numerical methods for solving the heat equation.

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