# Medical Image Analysis

#### CS 778 / 578

Computer Science and Electrical Engineering Dept. West Virginia University

February 14, 2011

CS 778 / 578 (West Virginia University) [Medical Image Analysis](#page-43-0) February 14, 2011 1/44

B

<span id="page-0-0"></span> $299$ 

 $\left\{ \begin{array}{ccc} 1 & 0 & 0 \\ 0 & 1 & 0 \end{array} \right.$ 

### **Outline**



#### [Internal forces](#page-8-0)

[Image-based forces](#page-16-0)

#### **[Constraints](#page-22-0)**

5 [Numerical implementation](#page-26-0)





 $\leftarrow$   $\Box$   $\rightarrow$ 

14.1 舌

## **Outline**



#### [Internal forces](#page-8-0)

- [Membrane spline energy](#page-11-0)
- [Thin-plate spline energy](#page-13-0)
- 3 [Image-based forces](#page-16-0)
- **[Constraints](#page-22-0)**
- 5 [Numerical implementation](#page-26-0)
- **[Weaknesses](#page-32-0)**
- [Extensions to the original paper](#page-34-0)

4. 0. 3

41

<span id="page-2-0"></span> $QQ$ 

# Basic active contour behavior

An active contour (or snake) is an energy minimizing parametric curve which evolves according to external constraints and is influenced by image forces which pull it toward features of interest.

- The exact energy functionals involved will depend on which features are of interest.
- We will impose membrane and thin-plate spline smoothness constraints on the snakes, and also allow for user intervention.

# Energy Functional

Behavior is governed by the energy functional

$$
E_{\text{snake}}^* = \int_0^1 E_{\text{int}}(\nu(s)) + E_{\text{image}}(\nu(s)) + E_{\text{con}}(\nu(s)) \, ds
$$

- $\bullet$   $v(s)$  is the parametric curve
- $\bullet$   $E_{int}$  represents the smoothness constraints
- $E_{image}$  represents image data constraints
- $E_{con}$  represents user input

4 D F

# Internal Energy

A combination of membrane and thin-plate spline smoothness

$$
E_{int} = \frac{1}{2} (\alpha(s) ||v_s(s)||^2 + \beta(s) ||v_{ss}(s)||^2)
$$

- This model allows the weights  $\alpha$ ,  $\beta$  to vary along the length of the curve.
- Setting  $\beta(s) = 0$  allows a discontinuity to develop at *s*.

 $209$ 

**K ロ ト K 何 ト K ヨ ト K** 

#### Definition

**Parametric Curve**: A vector valued function from some interval of the real line to Euclidean space.

<span id="page-6-0"></span>
$$
c(p) = \left[ \begin{array}{c} x(p) \\ y(p) \end{array} \right]
$$

where  $p \in [a, b]$ .

If  $c(a) = c(b)$  the curve is **closed**. If  $||c'(p)|| = 1$  the curve is **parameterized by arclength**.

# Tangent and Normal vector

Unit Tangent Vector

$$
T(p) = \frac{c'(p)}{||c'(p)||}
$$

Unit Normal Vector

$$
N(p) = \frac{T'(p)}{||T'(p)||}
$$

 $T(p) \perp N(p) \rightarrow T(p) \cdot N(p) = 0.$ 

$$
N(p) = \left[ \begin{array}{c} -t_y \\ t_x \end{array} \right] \text{or} \left[ \begin{array}{c} t_y \\ -t_x \end{array} \right]
$$

E

 $299$ 

 $\mathbf{A} \equiv \mathbf{A} + \mathbf{A} \mathbf{B} + \mathbf{A} \equiv \mathbf{A} + \mathbf{A} \equiv \mathbf{A}$ 

## **Outline**



### [Internal forces](#page-8-0)

- [Membrane spline energy](#page-11-0)
- [Thin-plate spline energy](#page-13-0)

### 3 [Image-based forces](#page-16-0)

- **[Constraints](#page-22-0)**
- [Numerical implementation](#page-26-0)
- **[Weaknesses](#page-32-0)**



4. 0. 3

<span id="page-8-0"></span> $QQ$ 

In general, we may want to minimize a combination of the two energies:

$$
\alpha E_{MEM}(c) + \beta E_{TPS}(c) = \int_0^l \alpha ||c'(s)||^2 + \beta ||c''(s)||^2 ds
$$

We will show that the minimization conditions are

$$
-\frac{d}{ds}\alpha c'(s) + \frac{d^2}{ds^2}\beta c''(s) = 0
$$

$$
-\alpha c''(s) + \beta c'''(s) = 0
$$

CS 778 / 578 (West Virginia University) [Medical Image Analysis](#page-0-0) February 14, 2011 10 / 44

∍

 $2990$ 

# Variational Calculus

The conditions for minimizing

$$
\min_c \int_{\Omega} F(s, c(s), c'(s), c''(s)) ds
$$

are

$$
F_c - \frac{d}{ds} F_{c'(s)} + \frac{d^2}{ds^2} F_{c''(s)} = 0
$$

The evolution equation that will satisfy this condition when steady-state has been reached

$$
\frac{\partial c}{\partial t} = -F_c + \frac{d}{ds} F_{c'(s)} - \frac{d^2}{ds^2} F_{c''(s)}
$$

イロト イ押 トイヨ トイヨト

Membrane spline energy of c(s)

$$
E_{MEM}(c) = \int_0^L ||c'(s)||^2 ds = \int_0^L x'(s)^2 + y'(s)^2 ds
$$

For an arclength parameterization, minimizing  $E_{MEM}(c)$  is equivalent to minimizing the length of c.

Applying variational calculus to

$$
\min_{x(s),y(s)} \int_0^L x'(s)^2 + y'(s)^2 ds
$$

gives two Euler-Lagrange conditions

$$
\frac{d}{ds}(2x'(s)) = 0
$$
  

$$
\frac{d}{ds}(2y'(s)) = 0
$$

<span id="page-11-0"></span> $\Omega$ 

イロト イ押 トイヨ トイヨト

# Membrane spline energy of c(s)

The Euler-Lagrange conditions can be rewritten as

$$
c''(s)=0
$$

The evolution equation

$$
\frac{dc}{dt} = \frac{d^2c}{ds^2} = \kappa N
$$

is also known as the geometric heat equation.  $\kappa$  is the curvature of the curve,  $||c''(s)||$ .

# Thin-plate spline energy of c(s)

$$
E_{TPS}(c) = \int_0^L ||c''(s)||^2 ds = \int_0^L x''(s)^2 + y''(s)^2 ds
$$

For an arclength parameterization, minimizing  $E_{TPS}(c)$  is equivalent to minimizing the square curvature of c.

The conditions for minimizing

$$
\min_c \int_{\Omega} F(s, c(s), c'(s), c''(s)) ds
$$

are

$$
F_c - \frac{d}{ds} F_{c'(s)} + \frac{d^2}{ds^2} F_{c''(s)} = 0
$$

The conditions for minimizing  $E_{TPS}(c)$  are

$$
c^{\prime\prime\prime\prime}(s)=0
$$

<span id="page-13-0"></span> $\Omega$ 

# Constant Coefficients  $\alpha$ ,  $\beta$ Minimizing snake energy

min *x*(*s*),*y*(*s*)  $\int_1^1$ 0 1  $\frac{1}{2}\alpha(x'(s)^2 + y'(s)^2)$  $+\frac{1}{2}$  $\frac{1}{2}\beta(x''(s)^2 + y''(s)^2)$  $+ E_{ext}(x(s), y(s)) ds$ 

The conditions for minimization are

$$
-\alpha x_{ss} + \beta x_{ssss} + \frac{\partial E_{ext}}{\partial x} = 0
$$
  

$$
-\alpha y_{ss} + \beta y_{ssss} + \frac{\partial E_{ext}}{\partial y} = 0
$$

The evolution equation is

$$
\frac{\partial v}{\partial t} = \alpha v_{ss} - \beta v_{ssss} - \nabla E_{ext}
$$

# Non-Constant Coefficients  $\alpha(s)$ ,  $\beta(s)$

Minimize  $E_{int} + E_{ext}$  with respect to  $x(s)$  and  $y(s)$ :

$$
\min_{x(s), y(s)} \int_0^1 \frac{1}{2} \alpha(s) (x'(s)^2 + y'(s)^2) + \frac{1}{2} \beta(s) (x''(s)^2 + y''(s)^2) + E_{ext}(x(s), y(s)) \ ds
$$

The conditions are

$$
-\frac{\partial}{\partial s}(\alpha(s)x'(s)) + \frac{\partial^2}{\partial s^2}(\beta(s)x''(s)) + \frac{\partial E_{ext}}{\partial x} = 0
$$
  

$$
-\frac{\partial}{\partial s}(\alpha(s)y'(s)) + \frac{\partial^2}{\partial s^2}(\beta(s)y''(s)) + \frac{\partial E_{ext}}{\partial y} = 0
$$

舌

<span id="page-15-0"></span> $2990$ 

# **Outline**

[Basic active contour behavior](#page-2-0) • [Geometry of curves](#page-6-0)

#### [Internal forces](#page-8-0)

- [Membrane spline energy](#page-11-0)
- [Thin-plate spline energy](#page-13-0)

### 3 [Image-based forces](#page-16-0)

- **[Constraints](#page-22-0)**
- [Numerical implementation](#page-26-0)
- **[Weaknesses](#page-32-0)**
- [Extensions to the original paper](#page-34-0)

4. 0. 3

<span id="page-16-0"></span> $\mathcal{A}$  . **FREE** 

- The **image** is a mapping  $I: R^2 \to R$ .
- The **curve** is a mapping  $v: R \to R^2$ .
- We may form composite functions from these two mappings

#### For example:

- $I(v(p))$  is the intensity of the image at the point  $v(p)$  on the curve.
- $\bullet$   $\nabla I(v(p))$  is the image gradient at the point  $v(p)$  on the curve.

Consider the weighted sum of two energy terms:

$$
E_{image} = w_{line} E_{line} + w_{edge} E_{edge}
$$

We will ignore the termination functional from the paper.

 $\Omega$ 

## Line Functional

$$
w_{line}E_{line} = w_{line}I(v(s))
$$

- if  $w_{line} > 0$  the snake will be attracted to dark contours
- $\bullet$  if  $w_{line} < 0$  the snake will be attracted to light contours

4 0 8 4

 $\overline{m}$   $\rightarrow$   $\rightarrow$ 

∍

ヨメ イヨ

# Edge Functional

$$
E_{edge(1)} = -||\nabla I(v(s))||^2
$$

The snake will be attracted to large image gradients.

B

ヨメ イヨ

**4 ロ ト 4 何 ト 4** 

# Scale Space

- We can use scale space to enlarge the convergence region of the snake.
- Recall that linear scale spaces result in blurred edges at coarse scales.
- This will propagate edge information far from the edge.

$$
E_{edge(2)} = -||\nabla(G_{\sigma} * I(v(s)))||^2
$$

4 D F

<span id="page-20-0"></span> $\Omega$ 

### Marr-Hildreth

Edges : zero crossings of the Laplacian ( $\nabla^2 = I_{xx} + I_{yy}$ )



<span id="page-21-0"></span>
$$
E_{edge(3)} = (G_{\sigma} * \nabla^2 I(v(s)))^2
$$

The snake will be attracted to zero crossings of the [sm](#page-20-0)[o](#page-22-0)[ot](#page-20-0)[he](#page-21-0)[d](#page-22-0)[L](#page-16-0)[a](#page-22-0)[p](#page-22-0)[la](#page-15-0)[c](#page-16-0)[i](#page-21-0)a[n.](#page-0-0)

CS 778 / 578 (West Virginia University) [Medical Image Analysis](#page-0-0) February 14, 2011 22/44

## **Outline**

[Basic active contour behavior](#page-2-0) • [Geometry of curves](#page-6-0)

#### [Internal forces](#page-8-0)

- [Membrane spline energy](#page-11-0)
- [Thin-plate spline energy](#page-13-0)

### 3 [Image-based forces](#page-16-0)

- **[Constraints](#page-22-0)**
- [Numerical implementation](#page-26-0)
- **[Weaknesses](#page-32-0)**
- [Extensions to the original paper](#page-34-0)

4. 0. 3

<span id="page-22-0"></span> $\mathbf{h}$  $\mathcal{A}$  . **FREE** 

# User Applied Constraints

### Spring Energy

The user may connect virtual springs between fixed point *p* , and contour position *v*:

$$
E_{spring} = k||p - v||^2
$$
  
=  $k((p_x - x)^2 + (p_y - y)^2)$ 

where k is a constant (spring stiffness)

$$
\nabla E_{spring} = \left[ \begin{array}{c} -2k(p_x - x) \\ -2k(p_y - y) \end{array} \right] = -2k(p - v)
$$

In the evolution equation

$$
\frac{\partial v}{\partial t} = \alpha v_{ss} - \beta v_{ssss} - \nabla E_{ext}
$$

the CS 778 / 578 (West Virginia University) *v v v v performance Analysis* February 14, 2011 24 / 44

# User Applied Constraints

### Repulsive Energy

Forces *v* away from fixed position *p*:

$$
E_{repulsion} = \frac{1}{||p - v||} = \frac{1}{\sqrt{(p_x - x)^2 + (p_y - y)^2}}
$$

$$
\frac{\partial E_{repulsion}}{\partial x} = (p_x - x)((p_x - x)^2 + (p_y - y)^2)^{-\frac{3}{2}}
$$
  

$$
\frac{\partial E_{repulsion}}{\partial y} = (p_y - y)((p_x - x)^2 + (p_y - y)^2)^{-\frac{3}{2}}
$$

**何 ) ( ヨ ) ( ヨ** 

4 0 8 4

 $\Rightarrow$ 

# User Applied Constraints

$$
\frac{\partial E_{repulsion}}{\partial x} = (p_x - x)((p_x - x)^2 + (p_y - y)^2)^{-\frac{3}{2}}
$$
  

$$
\frac{\partial E_{repulsion}}{\partial y} = (p_y - y)((p_x - x)^2 + (p_y - y)^2)^{-\frac{3}{2}}
$$

$$
\nabla E_{repulsion} = \frac{1}{r^2} \frac{p - v}{r}
$$

where  $r = ||p - v||$ . In the evolution equation, this term pushes *v* in the direction  $v - p$  with magnitude  $\frac{1}{r^2}$ .

舌

イロト イ押 トイヨ トイヨ

## **Outline**

[Basic active contour behavior](#page-2-0) • [Geometry of curves](#page-6-0)

#### [Internal forces](#page-8-0)

- [Membrane spline energy](#page-11-0)
- [Thin-plate spline energy](#page-13-0)

#### 3 [Image-based forces](#page-16-0)

**[Constraints](#page-22-0)** 

### 5 [Numerical implementation](#page-26-0)

#### **[Weaknesses](#page-32-0)**



4. 0. 3

<span id="page-26-0"></span> $\mathcal{A}$  . **FREE** 

# Discretized Curve

Store the curve as a vector of samples of  $v(s)$  at evenly spaced intervals in *s*. For  $v(s) = (x(s), y(s)),$ 

$$
\mathbf{x}_i = x(ih) \n\mathbf{y}_i = y(ih)
$$

where *h* is the parameter step size.

Compute derivatives of  $v(s)$  using finite difference formulas.

 $\Omega$ 

イロト イ押 トイヨ トイヨ

# For non-constant  $\alpha(s)$ ,  $\beta(s)$

$$
-\frac{\partial}{\partial s}(\alpha(s)x'(s)) + \frac{\partial^2}{\partial s^2}(\beta(s)x''(s)) + \frac{\partial E_{ext}}{\partial x} = 0
$$
  

$$
-\frac{\partial}{\partial s}(\alpha(s)y'(s)) + \frac{\partial^2}{\partial s^2}(\beta(s)y''(s)) + \frac{\partial E_{ext}}{\partial y} = 0
$$

Witkin, Kass, Terzopoulos discretize the Euler-Lagrange equations at this point.

First, they discretize  $(x', x'', y', y'')$  using backward and central differences:

$$
-\frac{\partial}{\partial s}(\alpha(s)(x_i - x_{i-1})) + \frac{\partial^2}{\partial s^2}(\beta(s)(x_{i-1} - 2x_i + x_{i+1})) + f_x(i) = 0
$$
  

$$
-\frac{\partial}{\partial s}(\alpha(s)(y_i - y_{i-1})) + \frac{\partial^2}{\partial s^2}(\beta(s)(y_{i-1} - 2y_i + y_{i+1})) + f_y(i) = 0
$$

 $QQ$ 

**K ロ ト K 何 ト K ヨ ト K** 

Then, they discretize  $(\frac{\partial}{\partial s}, \frac{\partial^2}{\partial s^2})$  $\frac{\partial^2}{\partial s^2}$ ) using forward and central differences:

$$
- (\alpha_{i+1}(x_{i+1} - x_i) - \alpha_i(x_i - x_{i-1}))
$$
  
+  $\beta_{i-1}(x_{i-2} - 2x_{i-1} + x_i)$   
-  $2\beta_i(x_{i-1} - 2x_i + x_{i+1})$   
+  $\beta_{i+1}(x_i - 2x_{i+1} + x_{i+2})$   
+  $f_x(i) = 0$ 

By doing the same for *y*, we can write two linear systems for the snake model...

イロト イ押 トイヨ トイヨ

 $QQ$ 

The two Euler-Lagrange equations can be written in matrix form

$$
Ax + f_x(x, y) = 0
$$
  
\n
$$
Ay + f_y(x, y) = 0
$$

where *A* is  $(n \times n)$  sparse matrix with 5 nonzero diagonals.

- A represents the smoothness of the curve
- $\bullet$   $f_x, f_y$  represent the external forces

The system of evolution equations is

$$
\frac{\partial x}{\partial t} = -Ax - f_x(x, y)
$$
  

$$
\frac{\partial y}{\partial t} = -Ay - f_y(x, y)
$$

 $\Omega$ 

 $\mathbb{R}^d \times \mathbb{R}^d \to \mathbb{R}^d \times \mathbb{R}^d$ 

4 0 8

# The linearized evolution equation

The authors present a mixed explicit/implicit method: implicit with respect to internal forces, and explicit with respect to external forces. Writing the finite difference in time as  $\gamma(v^t - v^{t-1})$ 

$$
Ax^{t} + f_{x}(x^{t-1}, y^{t-1}) = -\gamma(x^{t} - x^{t-1})
$$
  
\n
$$
Ay^{t} + f_{y}(x^{t-1}, y^{t-1}) = -\gamma(y^{t} - y^{t-1})
$$

These equations can be rewritten as

$$
(A + \gamma I)x^{t} = \gamma x^{t-1} + f_{x}(x^{t-1}, y^{t-1})
$$
  

$$
(A + \gamma I)y^{t} = \gamma y^{t-1} + f_{y}(x^{t-1}, y^{t-1})
$$

 $(A + \gamma I)$  is constant over time, so this matrix may be factorized/inverted once.

 $\Omega$ 

K ロ K K 個 K K ヨ K K ヨ K

## **Outline**

[Basic active contour behavior](#page-2-0) • [Geometry of curves](#page-6-0)

#### [Internal forces](#page-8-0)

- [Membrane spline energy](#page-11-0)
- [Thin-plate spline energy](#page-13-0)

### 3 [Image-based forces](#page-16-0)

- **[Constraints](#page-22-0)**
- 5 [Numerical implementation](#page-26-0)

### **[Weaknesses](#page-32-0)**



4. 0. 3

<span id="page-32-0"></span> $\mathbf{h}$ 14.1 **FREE** 

### Weaknesses

- Snakes are prone to getting stuck in local minima (they only see local image data)
- Topologically limited
- Only a 2D model
- Parameterization dependent
- Snakes may self-intersect, or become degenerate.

4 D F

 $\Omega$ 

# **Outline**

- [Basic active contour behavior](#page-2-0) • [Geometry of curves](#page-6-0)
- [Internal forces](#page-8-0)
	- [Membrane spline energy](#page-11-0)
	- [Thin-plate spline energy](#page-13-0)
- 3 [Image-based forces](#page-16-0)
- **[Constraints](#page-22-0)**
- [Numerical implementation](#page-26-0)
- **[Weaknesses](#page-32-0)**



4. 0. 3

<span id="page-34-0"></span> $\mathcal{A}$  .

### Inflation Force

Also called the "Balloon model"

L. D. Cohen, "On active contour models and balloons", CVGIP: Image Understanding, 1991.

 $\nabla E = f(v(s))N(v(s))$ 

- The snake expands in the normal direction.
- *f* may be intensity-based, edge-based, or constant
- This force can push the snake past local minima of the energy functional

 $\Omega$ 

母 ト イヨ ト イヨ

# Adding mass to the snake

$$
\mu \frac{\partial^2 v}{\partial t^2} + \gamma \frac{\partial v}{\partial t} = \alpha v_{ss} - \beta v_{ssss} - \nabla E_{ext}
$$

- Introducing mass gives the model inertia.
- This model can overshoot local minima.
- Equilibrium when  $\frac{\partial^2 v}{\partial t^2}$  $\frac{\partial^2 v}{\partial t^2} = \frac{\partial v}{\partial t} = 0$

4. 0. 3

 $QQ$ 

# Reparameterization

$$
E_{param} = \int_{\Omega} (||v'(s)||^2 - c)^2 ds
$$

- $v'(s) \cdot v'(s) = 1$  for an arclength parameterization.
- This energy can maintain an arclength parameterization
- Some degeneracies can be avoided

Avoided in the level-set formulation by representing the curve/surface implicitly.

押 トスミ トスミン

 $ORO$ 

# Subdivision

Ivins, J., Porrill, J., "Statistical snakes: Active region models.", Proc. 5th British Machine Vision Conf., 1994.

also proposed by others.



- Add more sample points as  $v(s)$  grows longer.
- Reparameterize so that high curvature regions are samples more densely.

## T-snakes

McInerney, T. and Terzopoulos, D., "T-snakes: Topology adaptive snakes", Medical Image Analysis, 2000.



The level-set formulation is also topologically adaptive.

4. 0. 3

 $\Omega$ 

# Gradient Vector Field

- The gradient of *I* does not provide useful information when the image is smooth.
- We would like to know the direction to the nearest edge.



4 0 8

ヨコ イ

 $\Omega$ 

# Gradient Vector Field

Xu, C. and Prince, J.L., "Gradient Vector Flow: A New External Force for Snakes", CVPR, 1997.

The gradient vector field,  $\mathbf{g}(x, y) = [u(x, y), v(x, y)]$  minimizes the energy

$$
E_{gyf} = \int_{\Omega} \mu(u_x^2 + u_y^2 + v_x^2 + v_y^2) + ||\nabla I||^2 ||\mathbf{g} - \nabla I||^2 ds
$$

- First term: membrane spline smoothness on *u*, *v*.
- Second term: **g** is near  $\nabla I$  when  $||\nabla I||$  is large
- When  $||\nabla I||$  is small, the smoothness term dominates

# Gradient Vector Field

- $\bullet$  Determine the evolution equation for minimizing  $E_{\text{gyf}}$ .
- Given  $I(x, y)$  compute the gvf,  $g(x, y)$ .
- $\bullet$  Use  $g(x, y)$  in the evolution equation for  $v(s)$ .

$$
\frac{\partial v}{\partial t} = \alpha v_{ss} - \beta v_{ssss} + \mathbf{g}(v(s))
$$

4 D F

 $\Omega$ 

### Next Class

Level Set Methods : implicit active contours.

Read

Malladi, R., Sethian, J., Vemuri, B., "Shape Modeling with Front Propagation : A Level Set Approach.", IEEE PAMI, 1995.

<span id="page-43-0"></span>4 D F